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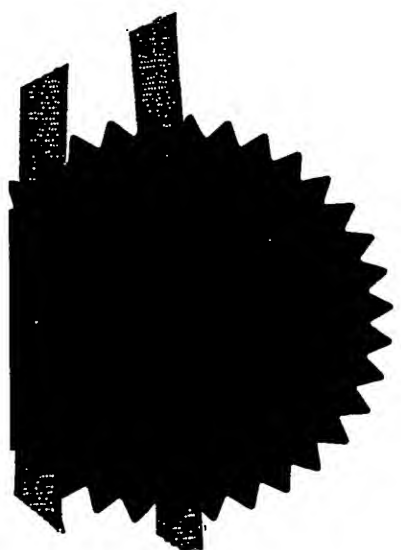
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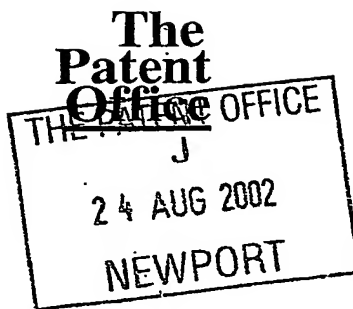
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Signed *Andrew Giersey*  
Dated 18 September 2003

Patent 1977  
(Rule 1)



1/77

# Request for grant of a patent

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1. Your reference P31821/JED/JAL 70:077 97a 997074: 057  
27AUG02 E743522-1 002481  
P01/7700 0.00-0219758.0

2. Patent Application Number (the Patent Office will fill in this part) 0219758.0 124 AUG 2002

3. Full name, address and postcode of the or of each applicant (underline all surnames) Grampian University Hospitals NHS Trust -and- University of Aberdeen  
Foresterhill House Kings College  
Ashgrove Road West Aberdeen  
Aberdeen AB24 3FX  
AB25 2ZB  
Patents ADP number (if you know it) 783670300 7131006002  
If the applicant is a corporate body, give the country/state of its incorporation United Kingdom

4. Title of the invention "Device"

5. Name of your agent (if you have one) Murgitroyd & Company  
"Address for service" in the United Kingdom to which all correspondence should be sent (including the postcode) 165 - 169 Scotland Street  
Glasgow  
G5 8PL  
Patents ADP number (if you know it) 1198015

6. If you are declaring priority from one or more earlier patent applications, give the country and the date of filing of the or of each of these earlier applications and (if you know it) the or each application number Country Priority application number (if you know it) Date of filing (day / month / year)

7. If this application is divided or otherwise derived from an earlier UK application, give the number and the filing date of the earlier application Number of earlier application Date of filing (day / month / year)

8. Is a statement of inventorship and of right to grant a patent required in support of this request? (Answer 'Yes' if:  
a) any applicant named in part 3 is not an inventor, or  
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Description 13

Claim(s) -

Abstract -

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Statement of inventorship and right to grant of a patent -

Request for preliminary examination and search (Patents Form 9/77) -

Request for substantive examination (Patents Form 10/77) -

Any other document (please specify) -

11. I/We request the grant of a patent on the basis of this application

Signature *MURGITROYD*  
MURGITROYD & COMPANY

Date 23/08/02

12. Name and daytime telephone number of person to contact in the United Kingdom  
Jamie Allan 01224 706616

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1     "Device"

2

3     This invention relates to an implantable replacement  
4     joint, and typically, but not exclusively to a body-  
5     implantable replacement joint to replace worn or  
6     damaged joints in a body.

7

8     Joint replacement is a well established practice for  
9     treating patients suffering from diseases such as  
10    inflammatory arthritis or osteoarthritis. These  
11    conditions can result in considerable pain, loss of  
12    function, deformity and loss of quality of life.

13   The most common types of artificial implant joints  
14   are used to replace worn or damaged hip joints, and  
15   typically consist of a ball and socket arrangement  
16   attached to bones at respective sides of the joint,  
17   or flexible silicon-based bridges such as the  
18   Swanson device, which is used for smaller joints  
19   such as the wrist or fingers. Loosening,  
20   dislocation tearing and fracture have been all  
21   reported for existing implants.

22

1 According to the present invention there is provided  
2 an implantable replacement joint comprising a first  
3 component for attachment to a first bone portion,  
4 and second component for attachment to a second bone  
5 portion, and a flexible component extending between  
6 the first and second components.

7  
8 The first bone portion is typically located on one  
9 side of a joint, and the second bone portion is  
10 typically located on the other side of the joint.

11  
12 The first and second components are typically  
13 adapted to be anchored within cavities in the  
14 respective first and second bone portions on  
15 opposing sides of the joint to be replaced. The  
16 first and second components can typically be  
17 anchored in place using friction, and in such  
18 embodiments can be shaped to be an interference fit  
19 within a cavity of the first and second bone  
20 portions. The cavity can be naturally occurring,  
21 e.g. the intramedullary canal, or can be created  
22 within a bone or group of bones to receive the first  
23 and second components, as required. In alternative  
24 embodiments, the first and second components can be  
25 anchored into the respective bone portions using  
26 adhesives, cement, grout, screw threads, or fixing  
27 devices such as screws, nails or expansion devices  
28 etc.

29  
30 In certain embodiments the first and second  
31 components have formations on their outer surfaces  
32 in order to key into the inner surfaces of the

1 cavities in the first and second bone portions. The  
2 formations on the outer surfaces of the first and  
3 second portions can typically be screw threads,  
4 annular or semi-annular ridges or simple protrusions  
5 or expansion fins on the outer surfaces.

6  
7 Typically the flexible component is elongate. In  
8 preferred embodiments, each of the first and second  
9 components has an elongate stem with a central bore  
10 extending along the stem to receive a part, e.g. one  
11 end, of the flexible component. In such  
12 embodiments, the flexible component can thus be  
13 substantially contained within a cavity formed by  
14 the central bores of the first and second  
15 components. Typically the cavity is longer than the  
16 flexible component, so that the flexible component  
17 can move axially within the cavity. Typically the  
18 bores of the first and second components are wider  
19 than the flexible component so that the flexible  
20 component is a loose fit within the cavity. The  
21 relative dimensions of the flexible component and  
22 the first and second components are preferably such  
23 that even if the first and second components are  
24 pushed together to close any gap between the central  
25 bores, the flexible component will not be compressed  
26 within the cavity by the first and second  
27 components.

28

29 In especially preferred embodiments, the first and  
30 second components have bearing surfaces that  
31 articulate against one another when the device is  
32 made up. Typically the central bores and the

1 flexible component extend through the bearing  
2 surfaces. The bearing surfaces can be arcuate and  
3 can be adapted to promote pivotal movements of the  
4 first and second components relative to one another.  
5 Preferably bearing surfaces promote particular  
6 pivotal movements e.g. in a particular plane.  
7 Typically the arcuate portions of the respective  
8 bearing surfaces on the first and second components  
9 are arranged on opposite axes, so that, for example,  
10 the bearing surface on the first component can be  
11 convex along an x-axis, and the bearing surface on  
12 the second component can be convex along a y-axis  
13 intersecting the x-axis. This arrangement can be  
14 extremely useful in promoting pivotal movements in  
15 more than one plane, allowing the replacement joint  
16 a number of degrees of freedom of movement, while  
17 controlling the location of the pivot axis on the  
18 device. However, it is envisaged that simple  
19 embodiments of the invention can be created with  
20 only one degree of freedom of movement, and without  
21 curved bearing surfaces.

22  
23 Typically the first and second components are made  
24 from a relatively hard plastics material or carbon  
25 fibre composites, and preferably from one that is  
26 not biodegradable. Suitable materials for the first  
27 and second components include stainless steel,  
28 alloys such as cobalt chrome or titanium alloy,  
29 polyethylene or other plastics materials, or  
30 ceramics or carbon fibre composites. It can be  
31 advantageous to use materials for the first and  
32 second components that have a similar modulus to

1 bone itself, and plastics materials are particularly  
2 useful in this respect.

3

4 The flexible component can be made from a resilient  
5 material such as rubber, and in preferred  
6 embodiments of the invention, the flexible component  
7 does have some resilience. The flexible component  
8 is typically formed from a relatively softer  
9 material than the first and second components. The  
10 flexible component can be made from e.g. silicone or  
11 polyurethane and can preferably have a flexibility  
12 that is intrinsic to the material used, although  
13 other forms of flexible component can be used where  
14 the flexibility is derived from e.g. a hinge  
15 inserted into a rigid material. The material chosen  
16 for the flexible portion is typically different from  
17 the material chosen for the first and second  
18 portions.

19

20 The flexible portion can typically have a convoluted  
21 hinge made up from a convoluted or folded section of  
22 the material.

23

24 In some embodiments of the invention, a bearing  
25 plate can be provided between the bearing surfaces  
26 of the first and second components. The bearing  
27 plate can typically be of a different material from  
28 the first and second components (for example, where  
29 the first and second portions are made from plastics  
30 material, the bearing plate can usefully be made  
31 from a metal), in order to reduce wear caused by the  
32 bearing surfaces of the first and second components



1 rubbing against one another. The bearing plate can  
2 have arcuate surfaces if desired, but in simple  
3 embodiments has generally flat faces. The bearing  
4 plate can extend the range of movement that is  
5 possible between the first and second components, by  
6 introducing an additional pivot point, so that each  
7 of the first and second components pivots on  
8 opposite faces of the bearing plate. The bearing  
9 plate can be formed with legs, extensions or  
10 prominent edges that can generally attach the  
11 bearing plate to one of the first and second  
12 components. The bearing plate could also be formed  
13 of plastics material, ceramics or other suitable  
14 materials. Where the first and second components  
15 are formed from ceramics materials, the bearing  
16 plate can comprise a plastics material so as to  
17 provide an interface of different materials at the  
18 bearing surfaces.

19  
20 The replacement joint of the invention is preferably  
21 a wrist joint, but can also be used in any joint,  
22 particularly fingers, toes, knees and elbows. Is  
23 particularly useful to replace worn or damaged  
24 joints where more than two degrees of freedom is  
25 required, such as rotation of the first and second  
26 components in addition to flexion/extension and  
27 medial/lateral deviation.

28  
29 In especially preferred embodiments of the  
30 invention, the pivot axis around which the first and  
31 second components move relative to one another is  
32 typically movable relative to the device, and this

1 is typically achieved by the ability of the flexible  
2 component to move within the bores of the first and  
3 second components, thereby creating a "sloppy hinge"  
4 between the first and second components. This  
5 permits the first and second components to move  
6 axially relative to one another while moving in  
7 relative rotation and flexion/extension or in  
8 medial/lateral directions. Indeed, the ability to  
9 move axially while rotating, deviating laterally,  
10 and flexing or extending enables the replacement  
11 joint to move in a similar fashion to the natural  
12 joint it is replacing. This reduces strain on the  
13 anchoring points between the bone portions and the  
14 first and second components, and reduces pull-out  
15 failures or bone wear at the interfaces.

16

17 An embodiment of the present invention will now be  
18 described by way of example, and with reference to  
19 the accompanying drawings, in which;

20

21 Fig 1 is a side view of a body implantable  
22 device;

23 Fig 2 is a front sectional view through the  
24 device of Fig 1;

25 Fig 3 is a side view of a first component of  
26 the fig 1 device;

27 Fig 4 is a front sectional view through the fig  
28 3 component;

29 Fig 5 is a front view of a second component of  
30 the Fig 1 device;

31 Fig 6 is a side sectional view through the fig  
32 5 component;

1        Fig 7 is a side view of a bearing plate used in  
2        the Fig 1 device;  
3        Fig 8 is a plan view of the bearing plate;  
4        Fig 9 is a side view of a flexible component of  
5        the Fig 1 device;  
6        Fig 10 is a perspective view of the Fig 1  
7        device;  
8        Fig 11 is a perspective view of the Fig 1  
9        device in flexion/extension;  
10       Fig 12 is a side view of the Fig 1 device in  
11       flexion/extension;  
12       Fig 13 is a perspective view of the Fig 1  
13       device showing lateral deviation;  
14       Fig 14 is a side view of the Fig 1 device  
15       showing lateral deviation;  
16       Fig 15 is a front view of the Fig 1 device  
17       showing lateral deviation;  
18       Fig 16 is a perspective view of the Fig 1  
19       device showing relative rotation of the two  
20       components; and  
21       Fig 17 is a side view of the Fig 1 device  
22       showing relative rotation of the two  
23       components.

24  
25       Referring now to the drawings, a body implantable  
26       device designed for use as the replacement wrist  
27       joint comprises a first component 5 and a second  
28       component 10. The first component 5 is dimensioned  
29       and adapted to be implanted within the distal end of  
30       the intramedullary canal of the radius, and the  
31       second component 10 is intended and adapted to be  
32       implanted into a bore created in the proximal part

1 of the carpus and/or metacarpals. Each of the first  
2 and second components 5,10 can have external  
3 protrusions such as ridges or screw-threads (not  
4 shown) to enhance retention of the component within  
5 the bone portion into which it is implanted. In  
6 this embodiment, each of the first and second  
7 components 5,10 is sized and adapted to fit within  
8 either the intramedullary canal of the radius or the  
9 bore created in the carpus and/or metacarpals and to  
10 form an interference fit within that cavity, so that  
11 they can be retained therein merely by friction  
12 between the outer surface of the components 5,10,  
13 and the inner surface of the cavity in the bone(s).  
14

15 With reference to fig 3 and fig 4, the first  
16 component 5 comprises a tapered stem 6 adapted to  
17 fit within the distal intramedullary canal of the  
18 radius, and a head 7 located on top of the stem 6.  
19 The head 7 has laterally extending arms and has a  
20 distal convex bearing surface 8 that is curved from  
21 the front of the first component 5 to the back. The  
22 radius of curvature of the surface 8 is  
23 approximately 16mm. The first component 5 has a  
24 blind-ended bore 9 extending axially through the  
25 stem 6, and presenting an aperture through the upper  
26 surface 8 of the head 7.  
27

28 The first and second components are made from ultra-  
29 high molecular weight polyethylene.  
30

31 With reference to Figs. 5 and 6 the second component  
32 10 also has a tapered stem 11, and a head 12, again

1 with laterally extending arms, and a proximal  
2 bearing surface 13. The proximal bearing surface 13  
3 of the head 12 is also convex, but is curved from  
4 one side of the second component 10 to the other  
5 side. The radius of curvature of the bearing face  
6 13 is approximately 65mm. The second component 10  
7 has a blind-ended bore 14 extending axially through  
8 the stem 11, and presenting an aperture through the  
9 upper surface 13 of the head 12.

10  
11 A flexible rod 15 of silicone as shown in fig 9 has  
12 a central cylindrical portion and tapered ends that  
13 are adapted to be received within the blind ended  
14 bores 9, 14 of the first and second components 5,10  
15 respectively. The length of the flexible rod is  
16 typically slightly less than the combined lengths of  
17 the blind ended bores 9, 14, so that when the device  
18 is assembled with the first and second components  
19 5,10 placed head-to-head, with the bores 9, 14  
20 aligned and the arms on the respective heads  
21 arranged parallel to one another, the flexible rod  
22 15 can move axially within the cavity formed by the  
23 two bores 9, 14.

24  
25 With reference to Figs. 7 and 8, a bearing plate 17  
26 formed of stainless steel is typically provided  
27 between the bearing surfaces 8, 13 of the heads  
28 7,12, and typically has an aperture 18 to allow  
29 passage of the flexible rod 15 through the bearing  
30 plate 17. The aperture 18 is aligned with the bores  
31 9,14 when the device is assembled. In this  
32 embodiment, the device is made up such that the

1 bearing surface 8 of the first component 5  
2 articulates against one surface 17a of the bearing  
3 plate 17, while the bearing surface 13 of the second  
4 component 10 articulates against the opposite  
5 surface 17b of the bearing plate 17. The bearing  
6 plate 17 typically has arms extending from the  
7 surface 17b plate to engage the side walls of the  
8 head 12 of the second portion 10. It will be  
9 appreciated that embodiments of the invention can  
10 function satisfactorily without a bearing plate 17,  
11 and that bearing plates can be used without side  
12 walls.

13  
14 Turning now to Figs. 10 to 17, the device is shown  
15 at rest in fig 10, with the two components 5,10 in  
16 axial alignment with one another with the bearing  
17 plate 17 interposed. In this configuration, the  
18 flexible rod 15 is not bent or energised in any way  
19 and is held within the cavity formed by the bores 9,  
20 14. Figs 11 and 12 show the device in flexion, with  
21 the second component 10 pivoting with respect to the  
22 first component 5 around the y-axis shown in fig 10.  
23 Notice that the bearing plate 17 moves with the  
24 second portion 10 relative to the first portion  
25 5, and that the bearing surface 8 of the head 7 of  
26 the first portion 5 articulates against the face 17a  
27 of the bearing plate 17. The front to back  
28 curvature of the bearing surface 8 promotes a smooth  
29 articulation about the y-axis. The ends of the  
30 flexible rod 15 remain within the bores 9, 14, and  
31 the central portion of the rod 15 bends to  
32 accommodate and control the flexion. Since the rod

1 15 can move axially within the cavity formed by the  
2 bores 9, 14, the pivot axis formed in the central  
3 portion of the rod 15 can move axially with respect  
4 to the first and second portions 5,10 as the device  
5 flexes, thereby allowing a greater range of movement  
6 of the joint. Also, since the flexible rod 15 can  
7 move within the cavity formed by the bores 9, 14,  
8 the two portions 5,10 can extend relative to one  
9 another along the x-axis, while undergoing flexion,  
10 extension, medial/lateral deviation and/or rotation.

11  
12 Figs 13, 14 and 15 show the joint moving in  
13 medial/lateral deviation around the z-axis of fig  
14 10, i.e. as if moving in radio-ulnar deviation when  
15 in place in the body. Notice that during lateral  
16 deviation around the z-axis, the bearing plate 17  
17 remains with the first portion 5, and the bearing  
18 surface 13 of the head 12 of the second portion 10  
19 articulates against the surface 17b of the plate 17.  
20 In pure lateral deviation, with no movement around  
21 the y-axis, the pivotal movement of the plate 17  
22 relative to the first portion 5 is negligible, and  
23 the lateral movement of the first portion 10 is  
24 constrained by the head 12 moving within the  
25 confines of the arms of the bearing plate 17. In  
26 certain circumstances, the plate 17 can move  
27 relative to the first portion 5, for example, when  
28 the flexible rod 15 moves axially to allow the  
29 extension of the device.

30  
31 Figs. 16 and 17 show relative rotational movement of  
32 the two portions 5,10 around the x-axis. Notice

1 that the arms of the bearing plate 17 keep the plate  
2 17 stationary with respect to the second portion 10,  
3 and the two portions pivot around the axis of the  
4 flexible rod 15 held straight within the central  
5 cavity formed by the bores 9, 14.

6  
7 Clearly is possible for the joint to carry out more  
8 complex combination movements involving a  
9 combination of rotation, medial/lateral deviation,  
10 and extension/flexion, in any combination. It is  
11 also possible for axial separation of the two  
12 portions to occur during any such movement.

13  
14 Modifications and improvements can be incorporated  
15 without departing from the scope of the invention ..

16



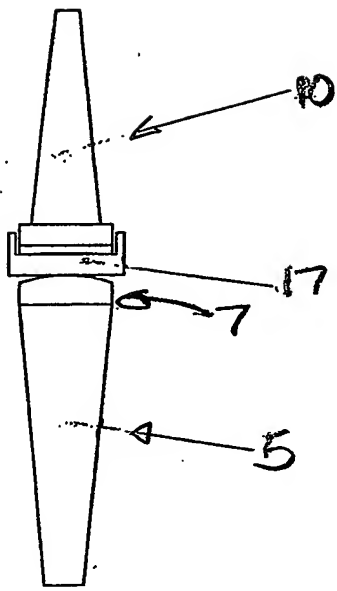


Figure 1

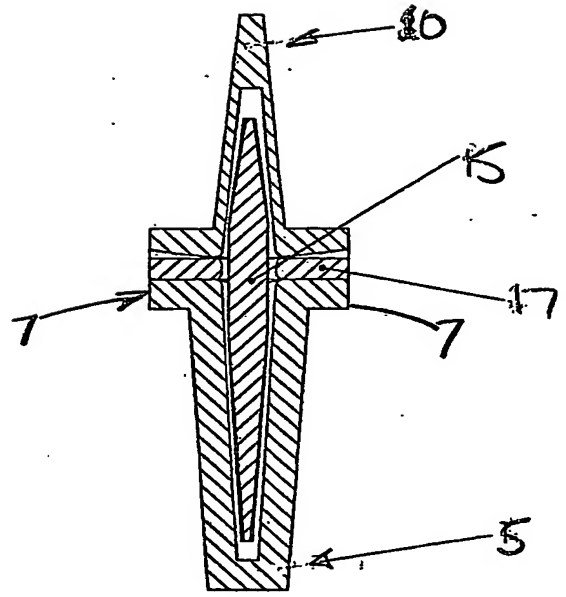


Figure 2

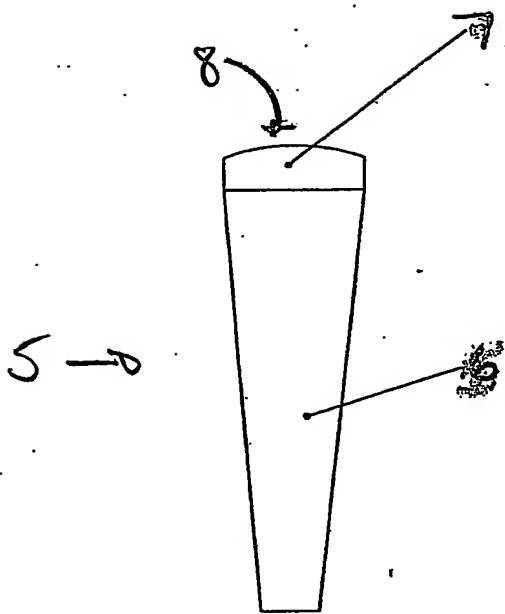


Figure 3

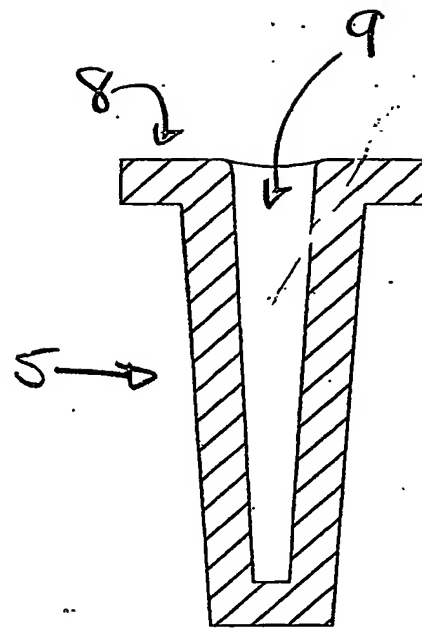


Figure 4

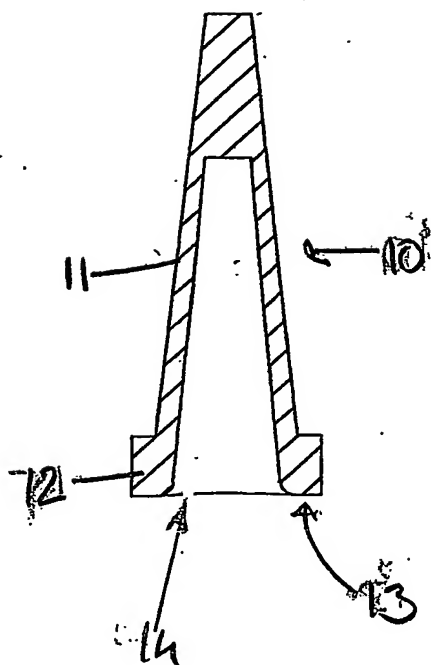


FIG. 6

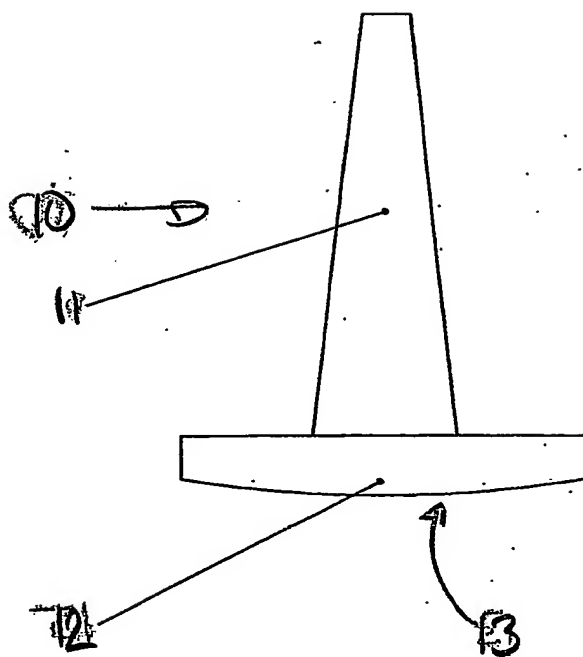


FIG. 5

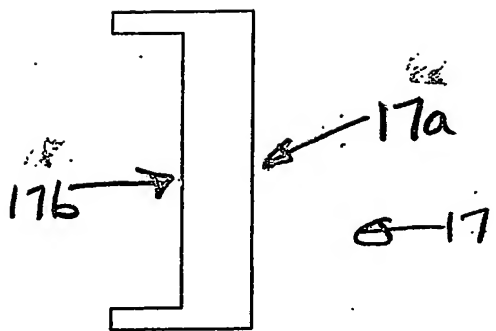


Figure 7

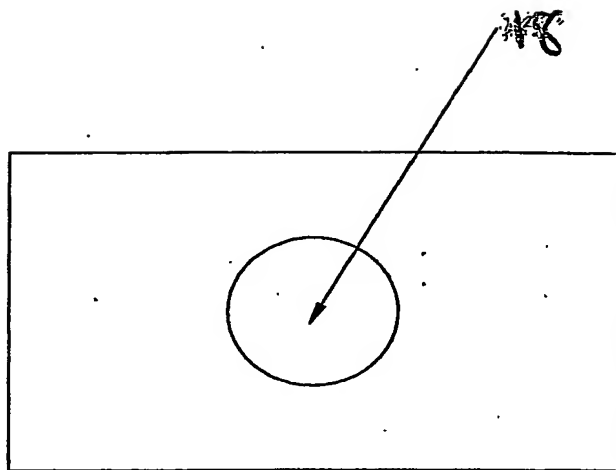


Figure 8

17

167



Figure 9

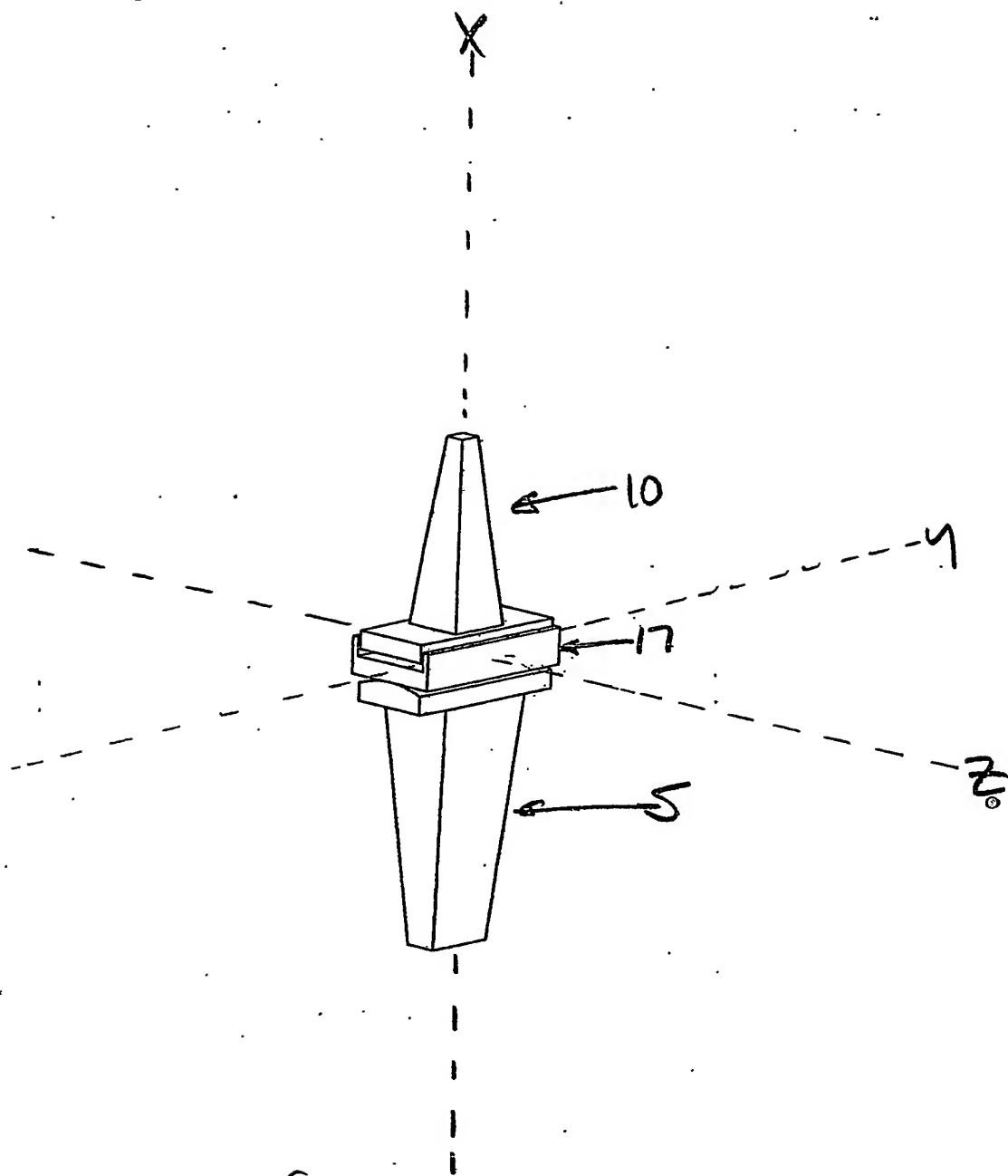


fig 10

NOT TO BE AMENDED

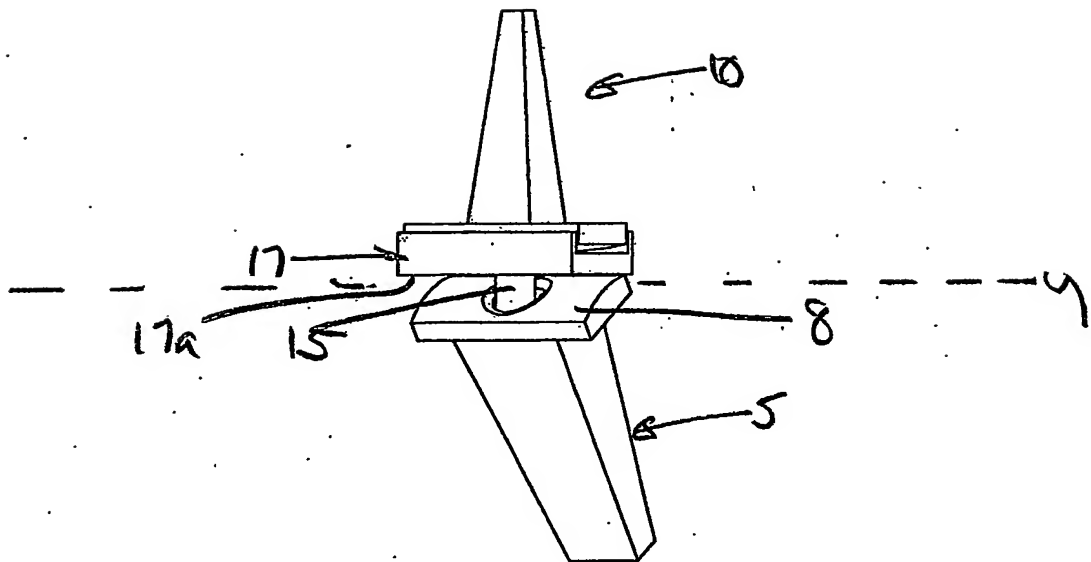


Fig 11

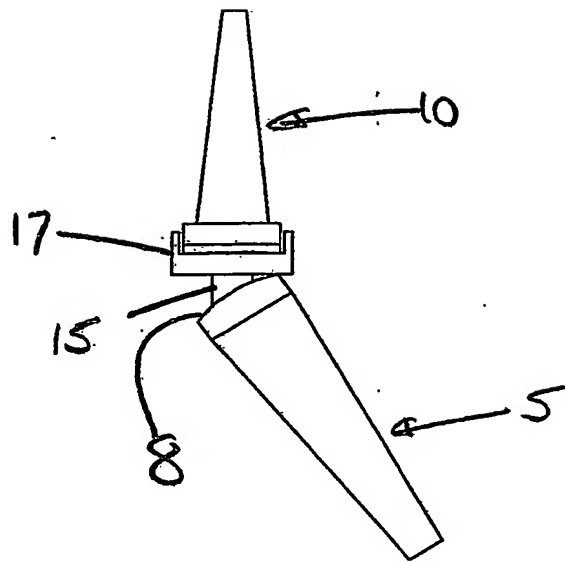


fig 12



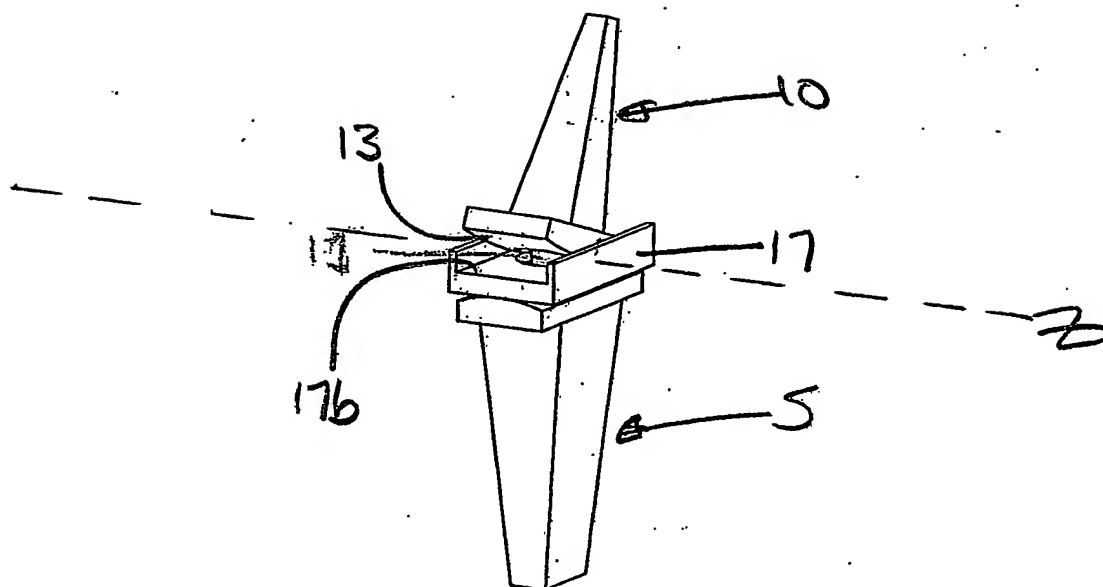


fig 13

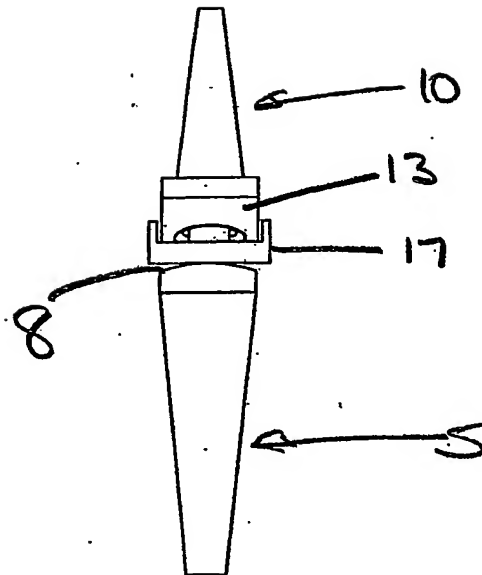


Fig. 14

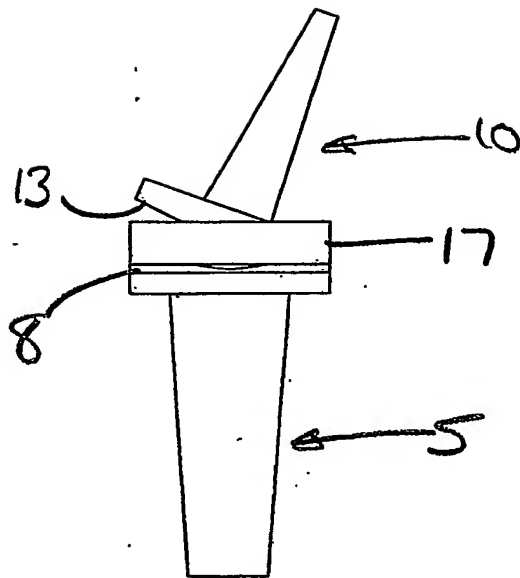


fig 15

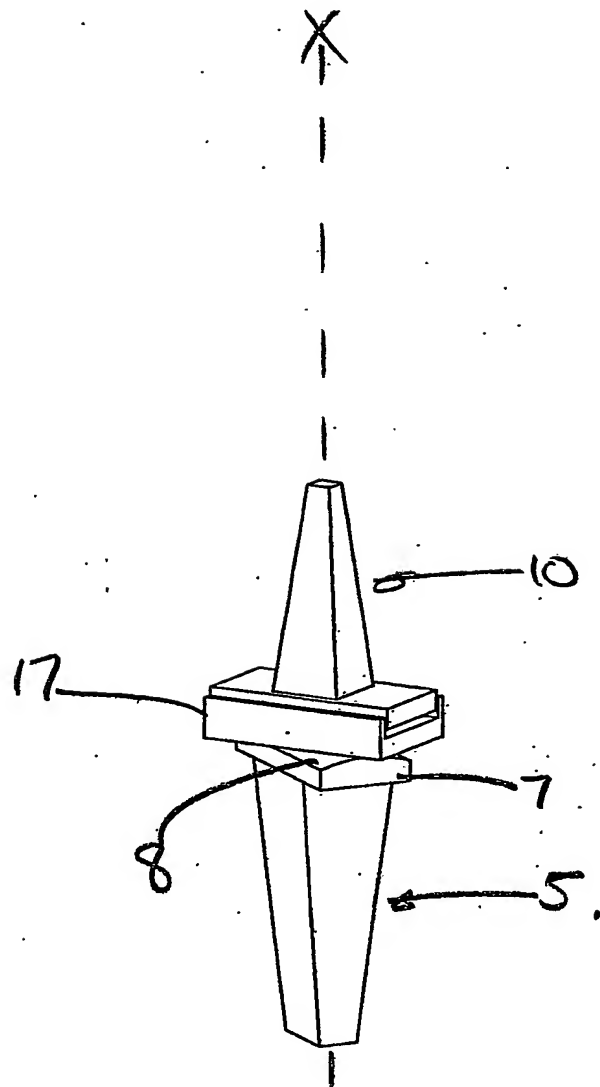


fig 6

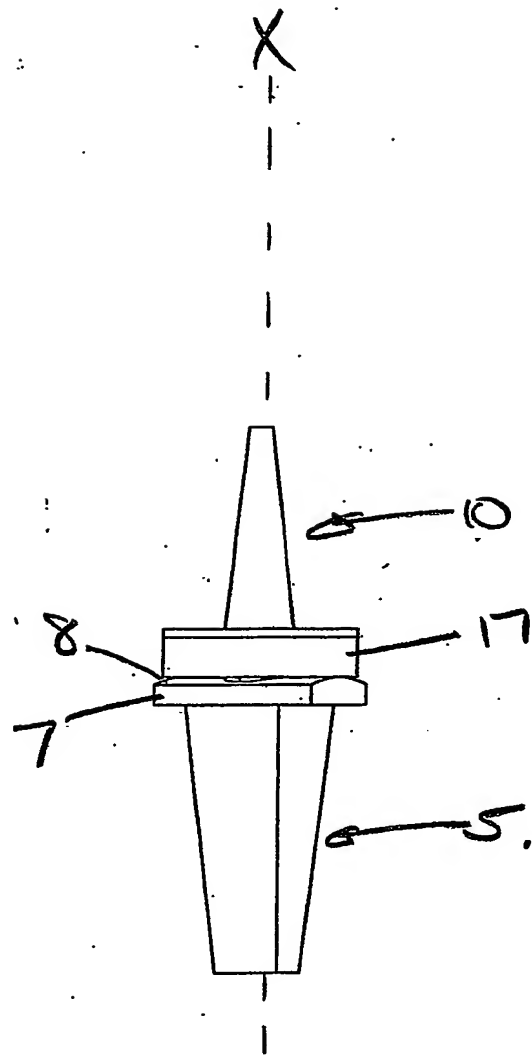


fig 17

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- ☒ **IMAGE CUT OFF AT TOP, BOTTOM OR SIDES**
- ☐ **FADED TEXT OR DRAWING**
- ☒ **BLURRED OR ILLEGIBLE TEXT OR DRAWING**
- ☐ **SKEWED/SLANTED IMAGES**
- ☐ **COLOR OR BLACK AND WHITE PHOTOGRAPHS**
- ☐ **GRAY SCALE DOCUMENTS**
- ☐ **LINES OR MARKS ON ORIGINAL DOCUMENT**
- ☐ **REFERENCE(S) OR EXHIBIT(S) SUBMITTED ARE POOR QUALITY**
- ☐ **OTHER:** \_\_\_\_\_

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